

# **MEMS for Glaucoma**

Thesis by

**Jeffrey Chun-Hui Lin**

In Partial Fulfillment of the Requirements

for the degree of

Doctor of Philosophy



CALIFORNIA INSTITUTE OF TECHNOLOGY

Pasadena, California

2012

(Defended February 6, 2012)

© 2012

Jeffrey Chun-Hui Lin

All Rights Reserved

To my family



## ACKNOWLEDGEMENTS

First, I would faithfully express my gratitude to my advisor, Prof. Yu-Chong Tai, who admitted me in 2005 to this fantastic Micromachining group at Caltech. Since I was a new Ph.D. graduate student at Caltech, Prof. Tai was an extremely good advisor to me during my years in the group. Prof. Tai is so knowledgeable that he could always foresee what I could not see in terms of the research, and therefore guide me on the right path to success. Every time when I felt frustrated about the experiments, he opened my eyes to the issues when I spoke to him, and I could always overcome the problems by incorporating his excellent ideas or advice. I always feel his enthusiasm about the research, and his optimism and confidence encouraged me to complete every tough experiment repeatedly. Under Prof. Tai's strict and complete trainings about the research, I started to understand something about this amazing MEMS world and make some working devices.

Prof. Tai has never let the students worry about the availability of research resources in the group. Undoubtedly, his vast knowledge and astute creativity has led the entire research team, and even the entire MEMS field, into the cutting-edge technologies and discoveries. Because of this, he is always able to maintain the whole research operation without stopping, even in such competitive academia today. Therefore, Prof. Tai can manage our research team as one of the top-leading MEMS research groups worldwide. Prof. Tai's attentive guidance and generous tolerance to the students, his desire and pursuit of new knowledge, and even his personality, are the best example for young researchers.

As I was a new international student, Dr. Tai became one of my best friends during my years at Caltech. In addition to academic research, Dr. Tai taught me a lot of important attitudes and necessary characteristics for me to lead a successful life in this new environment. I believe all the philosophy I have learned from him is as precious as the research results in the lab. It will accompany me and be my Holy Grail guiding me to success in my future life.

I would show my greatest appreciation to all my defense committee members, Prof. Joel Burdick, Prof. Changhui Yang, Prof. Azita Emami, and Prof. Hyuck Choo, for their instructive advice during my defense. I would especially like to thank Prof. Mark Humayun at Doheny Eye Institute at USC for his leading this wonderful glaucoma-management project. I was always stunned by his amazing skill in implanting devices. His clinical experiences always inspired me to improve the device designs. As a member of both the National Academy of Engineering and the Institute of Medicine, Prof. Humayun is a prodigy of learning and is an inspiring example for young academic researchers. His profound knowledge can always arouse the invention of new medical devices and therefore it makes me aspire to achieve the same level of expertise all the time. I would also specially thank my collaborative workers at USC, Dr. Rohit Varma and Dr. Salomeh Saati, for their assistance in the devices' animal trials and useful suggestions in terms of the device design.

I would like to thank our lab manager, Trevor Roper, for his endless maintenance of all kinds of facilities in the group as well as suggestions in terms of the device testing. With his sophisticated skill in repairing the equipment in the cleanroom, we always felt relieved when we saw Trevor working in the lab because Trevor is the person who calms

the fears of those who think they have to cease research due to equipment troubles. I would like to give thanks to our group administer, Christine Garske, for her kindly many aspects of the group, particularly for her big help in in managing group's purchasing orders. Christine always keeps track of every purchase order, ensuring that they are on schedule so that students have never to worry about the delay of getting the materials. She is very thoughtful to every group member. As a result, everything is well-ordered and goes smoothly under her organization. Besides, I very much appreciate our previous group administrator, Agnes Tong, for her help during my first few years in the group.

I would also like to say thanks to my lab-mates who joined the group with me in the same year, Ray Huang, Luca Giacchino, and Monty Nandra, for their useful help and constructive suggestions of my device fabrication and test. Working in a group with joint efforts and mutual support all towards the same goal of a Ph.D will be an unforgettable memory in my lifetime. I give special thanks to Po-Jui Chen, who was my mentor when I just joined the team and my co-worker when we worked together on the glaucoma-management project. Additionally, thanks to all previous and current group members in Caltech Micromachining Group for their assistance, encouragement, and tolerance. Working with the world's best group of students makes me aware of my insufficiencies and lack of capabilities in certain areas. It constantly pushes me to progress and pursue excellence in in all aspects of life. I would also like to thank all my talented SURF students, Brian Yu, Gilbert Lam, Rujian Chen, and Chenxi Qui, for their remarkable contribution and excellent jobs in the my experiments. It was so memorable to work with talented young undergrads like them in the lab during the summer. In short, I am pleased

to have worked and learned in one of the best MEMS research group worldwide and am extremely proud to be one of the group members among them.

I would like to express my great appreciation to my guitar teacher, Dr. Matthew Elgart, for instructing me in playing the classical guitar over the past few years. In addition to being a great performer, Matthew is also a very good teacher who has taught me from the start until now, and I can already perform some ensemble pieces. Matthew has always showed a lot of patience in explaining the music to me and helping me to choose the proper way to interpret it. It takes a lot of effort and different thoughts to crack every music piece and therefore playing a musical instrument actually helps me cultivate my concentration on lab work and perseverance on doing the research. Playing classical guitar enriches my life as a graduate student at Caltech and it is really a good stress reliever for the busy research life. Most importantly, Matthew's instruction satisfies my desire for understanding the classical guitar and even classical music. Thank Matthew for taking me into such a beautiful and amazing classical guitar world. I believe the classical guitar will be one of my best companions in my life.

I would like to thank all my friends who I became acquainted with at Caltech. It was so interesting to take the classes, work in the lab, and go to the Gym together with all them. Making so many friends from different countries really broadens my mind and views. In addition, I would like to thank all the Caltech Taiwanese students for their continuous support and help. In addition to the common discussions and suggestions about the research, it was always exciting to go grocery shopping with Taiwanese students at every Fri. night. I give particular thanks to the ACT (Association of Caltech Taiwanese) for holding all kinds of events during our traditional Taiwanese holidays such



as Chinese New Year, Dragon Boat Festival, and Mid-Autumn Festival, etc. Those events always made me feel warm during these holidays and not alone outside Taiwan.

I am grateful to my parents for their constant support of my decisions, and always encouraging me to pursue the best during my student's life. Their educating me as a person of integrity by setting themselves as examples, financially supporting me through my studies, and helping me make decisions all determine who I am now. I also feel so blessed for my parents-in-law's kindness, particularly for their unreserved support for my marriage with their daughter. Finally, I owe my dear wife, Yi-Ying Tang, for her continuous support and encouragement to me through several years. Although separated by a long distance for many years, Yi-Ying's tolerance and understanding has always been my firmest backbone giving me faith to proceed on and eventually fulfill the Ph.D. degree.

Finally yet importantly, I would like to thank my sweet Little-Turkey princess, Sharon Lin, who was born during my final last months of thesis writing period. My daughter's coming to the world makes me feel the miracle of life. Sharon's smile always cheers me up when I feel frustrated, and boosts me to work on my thesis and defense full steam ahead again.

Thank you to everyone who has given me helps in this exciting doctoral journey. Without you, this thesis would have not been possible.



# ABSTRACT

## MEMS for Glaucoma

Thesis by

**Jeffrey Chun-Hui Lin**

Doctor of Philosophy in Electrical Engineering

California Institute of Technology

Glaucoma is an eye disease that gradually steals vision. Open angle glaucoma is one of the most common glaucoma forms, in which eye fluid (aqueous humor) produced by the ciliary body cannot be drained away normally by patients' eyes. The accumulated eye fluid inside the anterior chamber causes high intraocular pressure (IOP), which is transmitted onto the retina in the back of the eyeball (globe), continuously suppressing and damaging the patient's optic nerves; this may lead to total blindness if not treated properly.

The current most-popular IOP monitoring technique is to use applanation tonometry, which applies applanation force onto the cornea and measures the resulting deformation in order to calculate the IOP. Even though applanation tonometry can provide quite useful information about patients' IOP, continuous monitoring of IOP is required for ophthalmologists to understand the IOP fluctuation of the patients, something which still cannot be achieved *via* current applanation approach. In addition, applanation tonometry requires skillful operation performed by well-trained professionals, such as ophthalmologists, making continuous IOP monitoring impractical.

In this work, we have developed a telemetric IOP sensor that is capable of monitoring IOP wirelessly and continuously. As the quality factor drops when a telemetric IOP sensor is implanted in the anterior chamber, due to the high loss tangent of the saline-based aqueous humor ( $\sim 0.2$ ) compared to air (0.0), a modified IOP sensor is developed to monitor IOP with sensing coil that is left exposed after implantation in order to avoid interruption from the eye fluid. Another approach is also proposed and tested to demonstrate that the quality factor can also be recovered by covering the sensing coil with low loss tangent materials.

Currently glaucoma is treated mostly by taking oral medications or applying eye drops. However, some glaucoma patients do not respond to those medications. Therefore, another physical approach, using a glaucoma drainage device (GDD), is necessary in order to drain out excessive eye fluid and serve as a long-term way to manage the increased IOP. Current commercially available glaucoma drainage devices do not have reliable valve systems to stop the drainage when the IOP falls into the normal range. Therefore, we have developed a dual-valved GDD to fulfill the “band-pass” flow regulation which drains out eye fluid only when IOP is higher than 20 mmHg, and stops drainage (closes the valve) when IOP is lower than 20 mmHg to prevent hypotony. The key component of GDD is a normally closed (NC) check-valve, which only opens to drain away the excess fluid when the pressure is higher than 20 mmHg. The proposed paradigm of our NC check-valve is to have a couple of parylene-C pre-stressed slanted tethers to provide the desired cracking pressure. The slanted tethers are achieved in this thesis by: 1) slanted photoresist generated by gray-scale photolithography, 2) pop-up mechanism, and 3) self-stiction bonding mechanism. The built-in residual tensile stress

can be controlled by mechanical stretching or thermal annealing. The protecting mechanism preventing the unwanted drainage when the eyes experience sudden unpredicted high IOP is achieved by utilizing a normally open (NO) check-valve. A “minimally invasive implantation” procedure is proposed in the thesis to implant the GDD subconjunctivally. The small size of the device allows its insertion using a #19-gauge needle.

To accurately design the desired cracking pressure and also predict the lifetime of the NC check-valve, parylene-C’s mechanical, thermal, and polymer properties are investigated. The results show that the properties of parylene-C are highly process-temperature-dependent and therefore can be tailored by adjusting the thermal annealing process.



# TABLE OF CONTENTS

<b>ACKNOWLEDGEMENTS .....</b>	<b>v</b>
<b>ABSTRACT .....</b>	<b>xi</b>
<b>TABLE OF CONTENTS .....</b>	<b>xv</b>
<b>LIST OF FIGURES .....</b>	<b>xxiii</b>
<b>LIST OF TABLES .....</b>	<b>xxxix</b>
<b>CHAPTER 1 INTRODUCTION.....</b>	<b>1</b>
1.1 INTRODUCTION TO GLAUCOMA.....	1
1.2 CURRENT TREATMENT OF PRIMARY OPEN ANGLE GLAUCOMA.....	2
1.2.1 Medications for glaucoma.....	2
1.2.2 Glaucoma filtration surgery .....	4
1.3 GLAUCOMA DRAINAGE DEVICE.....	4
1.3.1 Active glaucoma drainage device .....	4
1.3.2 Passive glaucoma drainage device.....	5
1.3.2.1 History of the development of glaucoma drainage devices	6
1.3.2.2 Contemporary passive glaucoma drainage device .....	9
1.3.2.3 Glaucoma drainage devices with no resistance .....	10
1.3.2.4 Glaucoma drainage devices with resistance .....	12
1.3.2.5 Comparison of current “tube-and-plate”-type glaucoma drainage devices.....	13
1.3.2.6 Postoperative complications of current glaucoma drainage devices.....	16

1.3.2.7 Long-term failure of the GDD: Bleb fibrosis .....	17
1.3.3 Proposed glaucoma drainage device design .....	18
1.4 INTRAOCULAR PRESSURE MONITORING .....	20
1.4.1 Current clinical IOP monitoring approaches .....	20
1.4.2 Wireless telemetric sensing technology .....	21
1.5 BIOCOMPATIBLE MATERIAL, PARYLENE-C, USAGE .....	23
1.6 CHARACTERISTICS OF PARYLENE-C .....	24
1.7 SUMMARY .....	26
<b>CHAPTER 2 PASSIVE NORMALLY CLOSED MICRO CHECK-VALVES .....</b>	<b>29</b>
2.1 OVERVIEW .....	29
2.2 THEORETICAL ANALYSIS OF NC MICRO CHECK-VALVES .....	32
2.2.1 Thin-film-flow theory of the check-valve .....	32
2.2.2 Calculation of the necessary pre-stress force .....	35
2.3 PRE-STRESSED SLANTED TETHER MICRO CHECK-VALVES .....	36
2.3.1 Slanted tether NC check-valve configuration .....	36
2.3.2 Thermal annealing pre-stressed NC check-valves .....	37
2.3.3 Sloped photoresist .....	38
2.3.3.1 One-time-exposure gray-scale photo-mask .....	38
2.3.3.2 Linearization of the sloped sacrificial photoresist .....	39
2.3.4 Fabrication .....	41
2.3.5 Device testing and discussion .....	44
2.4 INTEGRATION OF SLANTED TETHER CHECK-VALVES FOR HIGH-PRESSURE APPLICATIONS .....	47



2.4.1 Electrical-equivalent diode model .....	48
2.4.2 Multiple check-valve integration .....	48
2.4.3 Characterization results and discussion .....	51
2.5 POP-UP MICRO CHECK-VALVE.....	52
2.5.1 Pop-up micro check-valve device design .....	53
2.5.2 Device fabrication .....	54
2.5.3 Device characterization setup .....	58
2.5.4 Device characterization results .....	60
2.6 SELF-STICTION-BONDING MICRO NC CHECK-VALVES .....	62
2.6.1 Design concept of the self-stiction-bonding NC check-valve .....	62
2.6.2 Fabrication of the self-stiction-bonding NC check-valve .....	64
2.6.3 Characterization of the self-stiction-bonding NC check-valve.....	66
2.7 BLISTER TEST OF STICTION OF PARYLENE-C FILM .....	68
2.7.1 Experimental approaches .....	69
2.7.2 Theory of blister test .....	71
2.7.3 Blister test experimental setup .....	72
2.7.4 Testing results and discussion.....	74
2.7.5 Summary .....	78
2.8 SUMMARY AND CONCLUSION .....	79
2.8.1 Comparison of different types of micro check-valves .....	79
2.8.2 Lifetime of the slanted tether NC check-valves.....	81

## CHAPTER 3 INTEGRATION AND APPLICATIONS OF MICRO CHECK-

<b>VALVES FOR GLAUCOMA TREATMENT .....</b>	<b>83</b>
3.1 CONFIGURATION OF THE “BAND PASS” FLOW-RATE PROFILE DUAL-VALVE	
GDD SYSTEM .....	85
3.1.1 Dual back-to-back valves design .....	86
3.1.2 Numerical simulation of the glaucoma drainage device.....	87
3.2 DESIGN, FABRICATION, AND TEST OF THE NORMALLY OPEN VALVE.....	88
3.2.1 Design of the NO valve.....	88
3.2.2 Fabrication of the NO valve.....	90
3.2.3 Characterization of NO valve .....	91
3.3 SUTURELESS, MINIMALLY INVASIVE IMPLANTATION OF THE DUAL-VALVED	
GDD .....	93
3.3.1 Dual-valved GDD out-shape.....	94
3.3.2 Dual back-to-back valve configuration.....	94
3.3.3 Parylene-C protective tube carrier .....	95
3.3.4 Design and fabrication of the rollable/foldable parylene-C fixation	
anchors .....	96
3.3.5 Dual-valved glaucoma drainage device packaging.....	98
3.4 VALVE-POSITION-ADJUSTABLE DUAL-VALVED GDD.....	99
3.4.1 Configuration of the valve-position-adjustable dual-valved GDD	101
3.4.2 Grooved check-valves.....	102
3.4.3 Grooved check-valve fabrication procedures .....	103
3.4.4 Grooved check-valve packaging procedures .....	105

3.5 BENCH-TOP GDD CHARACTERIZATION.....	106
3.5.1 Bench-Top GDD characterization setup.....	106
3.5.2 Bench-Top GDD characterization results.....	107
3.6 GDD <i>EX VIVO</i> TEST AND DISCUSSION.....	109
3.6.1 GDD <i>ex vivo</i> implantation.....	110
3.6.2 Tapered hollow parylene-C protective tube mockup <i>ex vivo</i> implantation.....	111
3.7 SUMMARY AND CONCLUSION.....	114
<b>CHAPTER 4 HIGH-QUALITY-FACTOR PARYLENE-C-BASED     INTRAOcular PRESSURE SENSOR.....</b>	<b>117</b>
4.1 OVERVIEW.....	117
4.2 SENSING THEORY AND THE DEVICE DESIGN.....	125
4.2.1 Sensing scheme.....	125
4.2.2 Electrical and mechanical design of the device.....	126
4.3 DEVICE FABRICATION AND CHARACTERIZATION.....	128
4.3.1 Device fabrication.....	128
4.3.2 Device characterization.....	129
4.4 CHARACTERIZATION RESULTS AND DISCUSSIONS.....	131
4.5 QUALITY FACTOR RECOVERY STUDY.....	134
4.5.1 Overview.....	134
4.5.2 Q factor recovery by passivation layers of different materials.....	135
4.5.3 Q factor recovery by parylene-C passivation layers.....	138
4.5.4 Summary.....	141

4.6 SUMMARY AND CONCLUSION .....	142
<b>CHAPTER 5 CHARACTERISTICS OF PARYLENE-C FILM.....</b>	<b>145</b>
5.1 OVERVIEW .....	145
5.2 INTRODUCTION TO PARYLENE-C POLYMERIZATION .....	146
5.3 DENSIFICATION .....	147
5.3.1 Thickness-change measurement .....	149
5.3.2 In situ length-change measurement during thermal annealing .....	150
5.3.2.1 Length change under long-time thermal annealing process at 100°C .....	150
5.3.2.2 One cycle thermal annealing treatment.....	154
5.3.2.3 Cyclic thermal annealing treatment up to 120°C.....	155
5.3.3 Summary .....	158
5.4 OXIDATION .....	159
5.4.1 XPS .....	160
5.4.2 FTIR.....	163
5.4.3 Summary and discussion.....	167
5.5 CRYSTALLIZATION .....	169
5.5.1 X-ray diffraction method .....	171
5.5.1.1 In situ consecutive XRD scanning at 100°C.....	171
5.5.1.2 In situ temperature ramping annealing study.....	177
5.5.2 Time constant of parylene-C annealed at 100°C .....	180
5.5.3 Effect of deposition pressure difference .....	182
5.5.4 Summary and discussion.....	184

5.6 GLASS TRANSITION TEMPERATURE .....	186
5.6.1 Identification of glass transition temperature .....	188
5.6.1.1 Reported glass transition temperature of parylene-C.....	188
5.6.1.2 Ramping-temperature-dependent modulus experiment..	189
5.6.1.3 Dynamic mechanical analysis.....	193
5.6.2 Measuring results and discussion.....	197
5.6.3 Summary .....	207
5.7 UNIAXIAL TENSILE TEST.....	208
5.7.1 As-deposited parylene-C film .....	211
5.7.2 Deposition pressure influence.....	213
5.7.3 Oxidation effect .....	215
5.7.4 Annealing temperature and time influence .....	218
5.7.5 Effect of testing environmental temperature.....	221
5.7.6 Summary .....	225
5.8 RHEOLOGICAL PROPERTIES OF PARYLENE-C FILM .....	226
5.8.1 Creep of parylene-C.....	228
5.8.1.1 Creep overview .....	228
5.8.1.2 Introduction of the Burger's model.....	229
5.8.1.3 Primary and secondary creep of parylene-C.....	232
5.8.1.4 Summary .....	256
5.8.2 As-deposited parylene-C creep study under a step temperature profile.....	258
5.8.2.1 Experimental setup.....	258

5.8.2.2 Experimental results and discussions.....	260
5.8.3 Stress relaxation of parylene-C .....	265
5.8.3.1 Stress relaxation overview .....	265
5.8.3.2 Solution of the Burger’s model for stress relaxation .....	266
5.8.3.3 Stress relaxation experiment .....	267
5.8.3.4 Summary .....	271
5.8.4 Summary .....	272
5.9 VISCOPLASTICITY OF PARYLENE-C FILM AT HUMAN BODY TEMPERATURE ..	274
5.9.1 Overview of parylene-C viscoplasticity study.....	274
5.9.2 Sample preparation and viscoplastic experiments .....	275
5.9.2.1 Sample preparation and testing environment setup .....	275
5.9.2.2 Testing results .....	275
5.9.2.3 Discussion .....	276
5.9.3 Summary .....	282
5.10 SUMMARY AND CONCLUSION .....	282
<b>CHAPTER 6 GENERAL CONCLUSION .....</b>	<b>287</b>
<b>BIBLIOGRAPHY .....</b>	<b>293</b>

## LIST OF FIGURES

Figure 1-1: Molecular structure of parylene-C .....	23
Figure 2-1: Concept of the normally closed (NC) check-valve: (a) The check-valve is closed when the applied pressure $P$ is lower than the cracking pressure $P_c$ ; (b) the check-valve is open when the applied pressure $P$ is higher than the cracking pressure $P_c$ .....	30
Figure 2-2: Check-valve model for unsteady flow analysis: (a) side view, and (b) top view.....	32
Figure 2-3: Schematic of cracking-pressure-controlled parylene-C check-valve using the residual tensile stress in parylene-C after thermal annealing .....	36
Figure 2-4: A closer view of designed gray-scale photo-mask for the creation of sloped photoresist. The right pattern magnifies part of the pixel structure of the ring. ....	38
Figure 2-5: One-time-exposure gray-scale sacrificial photoresist profile: (a) before linearization, and (b) after linearization.....	41
Figure 2-6: Fabrication procedures. Slanted sacrificial photoresist is achieved using a one-time-exposure gray-scale photo-mask photolithography approach.....	42
Figure 2-7: SEM pictures of fabricated check-valves: (a) check-valves before photoresist removal, (b) a closer view of a tether and the sloped photoresist, (c) check-valves after photoresist removal, (d) a closer view of a tether after photoresist removal, (e) the cross-sectional view of the parylene-C anchor, and (d) micrograph of the top view of the check-valve .....	43

Figure 2-8: Testing setup for MEMS micro check-valves.....	44
Figure 2-9: Parylene-C tether width effect of the characterization results of thermally pre-stressed slanted tether micro check-valves: different tether widths but with the same annealing temperature at 100°C .....	45
Figure 2-10: Temperature effect of the characterization results of thermally pre-stressed slanted tether micro check-valves: different annealing temperatures but with the same tether widths of 50 $\mu\text{m}$ .....	46
Figure 2-11: Equivalent electrical circuit component model of check-valves: (a) one-diode model of one check-valve. $k$ and $dz$ are the spring constant of the tethers and the covering plate displacement, respectively. (b) In-series diodes model of in-series check-valves.....	49
Figure 2-12: Valve packaging: (a) A single valve packaged in capillary tubes and (b) four individual modules integrated using coupling tubes .....	50
Figure 2-13: (a) Modified device testing setup, (b) the characterization of single valve, and (c) the characterization of four check-valves in series.....	50
Figure 2-14: (a) Flow characteristics of a single valve, (b) micrograph of a check-valve in tube after testing, (c) flow characteristics of a four-check-valve assembly ..	52
Figure 2-15: The configuration of a pop-up check-valve. A close-up of the undercut parylene-C foot is shown in the circular area. ....	54
Figure 2-16: Fabrication procedures of (a) the pop-up micro check-valve, and (b) the testing chips .....	56



Figure 2-17: Micrograph of (a) 10 $\mu\text{m}$ undercut of the LOR30B, (b) top view of the NC check-valve, (c) top view of the outlet orifice, and (d) final device appearance .....	57
Figure 2-18: SEM pictures of (a) undercut parylene-C foot coating (back side view), (b) close view of undercut parylene-C foot coating, (d) normally closed check-valve, and (d) covering plate after pop-up .....	58
Figure 2-19: Cross section view of the testing chip with mounted in-channel check-valve .....	59
Figure 2-20: (a) Top view of the fabricated testing chip. (b) A close view of mounted device on top of the testing chip, sealed with dried photoresist .....	59
Figure 2-21: Captured pictures of normally closed pop-up check-valve during popping-up process (shown in arrow): (a) right before pop-up, (b) during pop-up, and (d) after pop-up. (Top parylene-C membrane is peeled off for clarity.) .....	61
Figure 2-22: Testing result of the pop-up check-valve .....	61
Figure 2-23: Schematics of the self-stiction-bonding NC check-valve .....	64
Figure 2-24: Fabrication procedures of the self-stiction-anchoring NC check-valve .....	65
Figure 2-25: Fabrication results of the self-stiction-anchoring NC check-valves: (a) SEM picture showing the regular NC check-valve, (b) SEM picture showing the NC check-valve with small holes for epoxy enhancement, (c) top view of the NC check-valve, and (d) NC check-valve with epoxy bonding enhancement .....	66
Figure 2-26: Pressure/flow-rate profile characterization results of the self-stiction-bonding NC check-valve .....	67

Figure 2-27: Top view of finished parylene-C check-valves fabricated for blister test ...	69
Figure 2-28: Fabrication procedures for circular parylene-C check-valve with different valve-seat surface treatments .....	70
Figure 2-29: Theoretical blister formation during experimentation: (a) The applied pressure is less than or equal to the critical debonding pressure, $P_c$ . (b) The applied pressure is higher than the critical debonding pressure, $P_c$ ; the parylene-C film starts to propagate.....	71
Figure 2-30: Experimental setup of the blister test: (a) the cross-section view of the test jig, and (b) schematic diagram of the testing setup .....	73
Figure 2-31: A typical curve of the blister test. The parylene-C film starts to debond when the applied pressure is higher than the critical debonding pressure.....	74
Figure 2-32: Stiction of parylene-C with different substrate surfaces after three kinds of releasing processes. Blue: acetone soak followed by IPA and water soak. Green: acetone soak followed by HF dip and water rinse. Red: soaking in mixture of acetone and silicone oil followed by direct air drying .....	75
Figure 2-33: Hydrogen bonding that occurs between water molecules and the passivated silicon surface. As the device dries, decreasing water content between the parylene-C film and the silicon pulls the two surfaces together through hydrogen bonding.....	76
Figure 2-34: Stiction between parylene-C and various surfaces after releasing in a mixture of acetone and silicone oil.....	77

Figure 2-35: Stiction between the parylene-C and the silicon surface is reduced due to the silicone oil layer, which reduces surface passivation and the proximity between surfaces.....	77
Figure 3-1: Concept of the “band pass” flow-rate profile of the proposed GDD system comprising (a) an NC check-valve, and (b) an NO valve to achieve (c) a band pass flow-rate profile .....	85
Figure 3-2: The cross section of a normally open check-valve .....	88
Figure 3-3: COMSOL Multiphysics™ simulation of the dual-valved GDD system: (a) deflection simulation of the NC check-valve, (b) flow-rate simulation results of the NC check-valve, (c) deflection simulation of the NO valve, (c) flow-rate simulation results of the NC check-valve, (e) flow-rate simulation of the dual-valved GDD system, (f) flow-rate simulation results of the dual-valved GDD system.....	89
Figure 3-4: Fabrication procedures of the NO valve .....	90
Figure 3-5: Fabrication results of the NO valve: (a) top view of the NO valve, and (b) SEM picture of the NO valve .....	91
Figure 3-6: Pressure/flow-rate profile characterization results of the NO valve .....	92
Figure 3-7: Concept of the minimally invasive implantation: (a) Subconjunctival implantation idea of the (GDD) implanted through the anterior chamber of the eye. (b) A complete GDD system consisting of a dual-valve micro-flow regulation system (one NC check-valve at one end of the tube and one NO valve on the other end of the tube), a parylene-C protective tube carrier, and a rollable/foldable anchor .....	93

- Figure 3-8: (a) Fabrication procedures of the parylene-C protective tube carrier, (b) coated 40  $\mu\text{m}$  parylene-C on the sacrificial capillary glass tubing, (c) slanted and completed parylene-C protective tube carrier..... 95
- Figure 3-9: Fabrication procedures of the parylene-C fixation anchors..... 98
- Figure 3-10: Packaging procedures of the dual-valved GDD system: (a) NC check-valve; (b) NO valve; (c) NC check-valve with stiction bonding enhanced by epoxy; (d) hollow parylene-C protective tube carrier; (e) one NC and one NO valve sealed in the parylene-C protective tube carrier (transparent glass tube used here for clarity); (f) anchors with trenches of 300  $\mu\text{m}$  in radius, different anchor shapes designed to facilitate the surgical convenience, and future GDD fixation (left: ragged anchor; middle: foldable anchor; right: rollable squeeze-tail anchor); (g) completed assembled GDD in top view; (h) anchors can be rolled/folded for testing and implantation convenience. Check-valves are first sealed in the carrier, which is then assembled onto anchors. .... 100
- Figure 3-11: Schematics of valve-in-tube system: (a) Combination of one NC valve and one NO valve with a coupling tube to form the micro-flow regulating assembly. (b) Final finished valve-in-tube system ..... 102
- Figure 3-12: Cross section of the grooved self-stiction-bonding NC check-valve design ..... 103
- Figure 3-13: Modification of step 4 of the fabrication procedures of (a) NC check-valve and (b) NO valve by DRIE to incorporate a circular groove using the same photoresist mask for parylene-C patterning (photoresist mask not shown) 103

- Figure 3-14: Micrographs of: (a) the fabrication result of an NC check-valve, (b) the top view of a NC check-valve packaged inside a coupling tube, (c) packaging results of the micro-flow regulating assembly, (d) the micro-flow regulating assembly packaged inside a tapered parylene-C protective tube carrier 610  $\mu\text{m}$  in diameter, suitable for a #19-gauge hypodermic needle ..... 104
- Figure 3-15: The packaging procedures: (a) one check-valve attached to one end of the coupling tube, (b) complete micro-flow regulating assembly, (c) final valve-in-tube system..... 105
- Figure 3-16: Testing setup of the GDD: Photoresist is painted in the gap between GDD and Teflon tubing for sealing..... 107
- Figure 3-17: Dual-valved GDD characterization results: The fluid starts to flow after 0.33 psi ( $\sim 17$  mmHg) and closes at 1.1 psi ( $\sim 57$  mmHg). Water was chosen as the working fluid..... 108
- Figure 3-18: Testing setup of GDD *ex vivo* implantation test ..... 110
- Figure 3-19: (a) The plunger in the needle introducer, (b) a GDD with folded zigzag type parylene-C fixation anchor inserted into a #19-gauge hypodermic needle, (c) a hollow parylene-C tube subconjunctivally implanted into an enucleated porcine eye, (d) testing dye shunted into the hollow tube. The drained-out testing dye is visible..... 111
- Figure 3-20: *Ex vivo* implantation results of: (a) GDD 1 and (b) GDD 2. The testing dye started to drain out after fluids were injected and stopped at 24 mmHg. (c) Residual dye kept flowing slightly at 4 mmHg. .... 113

- Figure 3-21: Inspection of the NC check-valve after *ex vivo* implantation: (a) right after the implantation, and (b) after one week of soaking in DI water ..... 114
- Figure 4-1: (a) Wireless sensing concept of implantable IOP sensor in the anterior chamber, (b) the glass reader paradigm, (c) a real IOP sensor *in vivo* tested in a rabbit eye..... 120
- Figure 4-2: The concept of the wireless inductive coupling link: The frequency shift is registered through an external oil reader. .... 121
- Figure 4-3: Resonant frequency shift corresponds to the applied pressure: (a) Frequency decreases as the capacitance increases; (b) No frequency shift is observed when no pressure difference exists; (c) Frequency increases as the capacitance decreases. .... 122
- Figure 4-4: The new IOP sensor design: (a) Top view of the sensing part, (b) AA' cross-section view of the IOP sensor ..... 122
- Figure 4-5: The newly designed IOP sensor is implanted at the pars plana with the implantation tube going through the choroid, while the sensing part still remains outside the choroid, but under the conjunctiva of the eye. .... 124
- Figure 4-6: Fabrication procedures of the sensing part of the IOP sensor..... 128
- Figure 4-7: IOP sensor fabrication and assembling results: (a) Completed sensing part, (b) implantation tube attached onto the backside of the sensing part concentric with the pressure access hole, (c) IOP sensor mounted to the testing tube by photoresist, (d) final IOP sensor..... 130

Figure 4-8: IOP sensor characterization setup: a 1.5-mm-diameter hand-wound coil served as the reader coil and a HP4195A network/spectrum analyzer was used to register the frequency shift of the phase dip. ....	131
Figure 4-9: Bench-top characterization results of the IOP sensor: the resonant frequency was 379 MHz when the applied pressure difference was 0 mmHg, and shifted to higher frequency when the pressure difference increased. ....	132
Figure 4-10: Sensitivity analysis of the IOP sensor. ....	133
Figure 4-11: The idea of covering the device with different passivation layers: glass cover slip, photoresist, or epoxy. The IOP sensor is shown in gray in the figure. ....	135
Figure 4-12: IOP sensors covered by two different materials with low loss tangent: (a) photoresist and (b) epoxy. ....	136
Figure 4-13: The idea of covering the device with several layers of parylene-C sheets. The IOP sensor is shown in gray in the figure. ....	139
Figure 4-14: Quality factor recovering results versus parylene-C thickness by covering the IOP sensor with several parylene-C layers. ....	140
Figure 4-15: Modified sensing coil fabrication procedures: After 30 $\mu\text{m}$ parylene-C layer is deposited on top of the capacitor metal plate, an extra oxygen plasma etching process is executed to thin down the central parylene-C to retain the capacitor sensitivity. ....	142
Figure 5-1: Measured thickness of 20 $\mu\text{m}$ parylene-C film annealed at 100°C in the convection oven. ....	149

Figure 5-2: (a) Obtained length change of the parylene-C film annealed at 100°C in air for 8 hours, and (b) a closer view of the length change during the first 2.5 minutes.....	152
Figure 5-3: Length change of the parylene-C film which was annealed at 100°C in air for 8 hours in the previous test. The sample was annealed again at 100°C for another 2 hours. ....	153
Figure 5-4: Length change of parylene-C film annealed under the temperature ramping rate at 3.33°C/min and its hypothesized phenomenon interpretation by dominant effect .....	155
Figure 5-5: Six cycles of thermal annealing of parylene-C film up to 120°C: The length of the film never goes back to its original length after the first-time thermal annealing.....	157
Figure 5-6: The parylene-C film behaves differently after the first-time thermal annealing.....	157
Figure 5-7: The oxidative species of parylene-C proposed by Nowlin [189].....	160
Figure 5-8: Typical XPS results of parylene-C samples. Top left: A closer view of the peak of 531.6 eV representing the content of oxygen .....	161
Figure 5-9: Comparison of two XPS results of parylene-C annealed at 200°C for two days in air and in vacuum .....	163
Figure 5-10: Typical FTIR results of parylene-C film. The black curve represents the as-deposited parylene-C film, while the others represent the results of annealing at 100°C. ....	165
Figure 5-11: FTIR results of parylene-C annealed at 200°C in air for different times...	166



Figure 5-12: Comparison of the FTIR results of parylene-C annealed at 200°C in air and vacuum, all for two days.....	167
Figure 5-13: Typical XRD scanning results showing curve from 10°–30°C .....	172
Figure 5-14: XRD results of in situ XRD measurement of parylene-C consecutively annealed at 100°C in helium.....	174
Figure 5-15: Crystallite size growing history of parylene-C annealed at 100°C in helium .....	176
Figure 5-16: XRD results of parylene-C annealed at 30°, 37°, 40°, and 50°C.....	178
Figure 5-17: XRD results of in situ XRD measurement of parylene-C consecutively annealed at different temperatures in helium. Temperature ramping rate = 3°C/min.....	179
Figure 5-18: Crystallite size growing history of parylene-C annealed at different temperatures in helium .....	180
Figure 5-19: The crystallite size versus the annealing time.....	181
Figure 5-20: Comparison of the results of XRD measurement of parylene-C deposited at 22 mT and 35 mT .....	184
Figure 5-21: Elastic modulus response versus temperature change .....	186
Figure 5-22: Concept of the ramping-temperature-dependent modulus experiment. Every peak represents one uniaxial tensile test.....	190
Figure 5-23: Elastic (Young's) modulus versus temperature curve. The transition region I represents the general glass transition region for as-deposited parylene-C, while transition region II represents the general glass transition region for parylene-C annealed at 100°C. ....	191

- Figure 5-24: The concept of dynamic analytical analysis. (a) A sinusoidal oscillatory stress is applied and the material's sinusoidal strain response with a phase delay (viscoelastic materials) is measured. (b) The relationship of complex modulus ( $E^*$ ), the storage modulus ( $E'$ ), and the loss modulus ( $E''$ ) ..... 194
- Figure 5-25: A typical DMA testing curve showing the results of storage modulus, loss modulus, and tan delta. Every curve has its corresponding definition to identify  $T_g$ . ..... 195
- Figure 5-26: A comparison of the results of the ramping-temperature-dependent modulus experiment and the DMA test. Parylene-C sample was annealed at 100°C for one day in vacuum.  $T_g$  is found at the inflection point of each glass transition region. .... 197
- Figure 5-27: Measured  $T_g$  of four parylene-C annealed in different conditions: 3 samples at 100°C, with as-deposited parylene-C as a comparison..... 201
- Figure 5-28: Measured  $T_g$  of parylene-C samples all annealed in 100°C but for different times: 30 sec, 1 min, 3 min, and 30 min ..... 202
- Figure 5-29: Measured  $T_g$  of four parylene-C samples annealed in different temperatures ..... 202
- Figure 5-30: Measured  $T_g$  of seven parylene-C samples annealed in different temperatures. Samples were annealed in the DMA Q800 chamber for 30 min prior to the  $T_g$  test. .... 203
- Figure 5-31: Typical as-deposited parylene-C film uniaxial tensile test results obtained by TA instrument DMA Q800 system. Toe region is compensated to give the

final correct calculated parameters. All terminologies follow the definition of the ASTM standard D882-09 and D638-08 [233, 234].	210
Figure 5-32: Comparison of parylene-C film deposited at different pressures. (a) Two stress-strain curves. (b) A closer view of elastic modulus and yield point.	215
Figure 5-33: Comparison of uniaxial tensile test results of parylene-C film with three different treatments: as-deposited, 1 day annealed at 100°C in air, and 1 day annealed in vacuum	216
Figure 5-34: Comparison of uniaxial tensile test results of parylene-C film with six different treatments	218
Figure 5-35: A closer view of Figure 5-34 (strain lower than 10%)	219
Figure 5-36: A series of uniaxial tensile tests of parylene-C performed at different environmental temperatures	223
Figure 5-37: A closer view of Figure 5-36 (strain lower than 5%)	223
Figure 5-38: A comparison of elastic modulus measured by DMA (as-deposited curve in Figure 5-27 in 5.6) and obtained from Table 5-13	224
Figure 5-39: Creep behavior of polymers: (a) constant applied stress during creep test at a constant temperature; (b) total strain versus time; (c) removal of the stress at the beginning of the creep recovery test; (d) recovery strain curve	229
Figure 5-40: Schematic diagram of the Burger's model	230
Figure 5-41 (a): Creep results of the as-deposited parylene-C deposited at 22 mTorr ( $T_g=53.4^\circ\text{C}$ ); (b): Stress relaxation results of the as-deposited parylene-C deposited at 22 mTorr ( $T_g=53.4^\circ\text{C}$ )	240

Figure 5-42 (a): Creep results of the as-deposited parylene-C deposited at 35 mTorr ( $T_g=55.1^\circ\text{C}$ ); (b): Stress relaxation results of the as-deposited parylene-C deposited at 35 mTorr ( $T_g=55.1^\circ\text{C}$ ) .....	242
Figure 5-43 (a): Creep results of the parylene-C annealed at $100^\circ\text{C}$ for 30 minutes in the convection oven ( $T_g=108.2^\circ\text{C}$ ); (b): Stress relaxation results of the parylene-C annealed at $100^\circ\text{C}$ for 30 minutes in the convection oven ( $T_g=108.2^\circ\text{C}$ )	244
Figure 5-44 (a): Creep results of the parylene-C annealed at $100^\circ\text{C}$ for 1 day in the convection oven ( $T_g=111.8^\circ\text{C}$ ); (b): Stress relaxation results of the parylene-C annealed at $100^\circ\text{C}$ for 1 day in the convection oven ( $T_g=111.8^\circ\text{C}$ ) .....	246
Figure 5-45 (a): Creep results of the parylene-C annealed at $100^\circ\text{C}$ for 1 day in the vacuum oven ( $T_g=113.1^\circ\text{C}$ ); (b): Stress relaxation results of the parylene-C annealed at $100^\circ\text{C}$ for 1 day in the vacuum oven ( $T_g=113.1^\circ\text{C}$ ).....	248
Figure 5-46 (a): Creep results of the parylene-C annealed at $100^\circ\text{C}$ for 2 days in the vacuum oven ( $T_g=115.2^\circ\text{C}$ ); (b): Stress relaxation results of the parylene-C annealed at $100^\circ\text{C}$ for 2 days in the vacuum oven ( $T_g=115.2^\circ\text{C}$ ) .....	250
Figure 5-47 (a): Creep results of the parylene-C annealed at $200^\circ\text{C}$ for 1 day in the vacuum oven ( $T_g>200^\circ\text{C}$ ); (b): Stress relaxation results of the parylene-C annealed at $200^\circ\text{C}$ for 1 day in the vacuum oven ( $T_g>200^\circ\text{C}$ ).....	252
Figure 5-48 (a): Creep results of the parylene-C annealed at $200^\circ\text{C}$ for 2 days in the vacuum oven ( $T_g>200^\circ\text{C}$ ); (b): Stress relaxation results of the parylene-C annealed at $200^\circ\text{C}$ for 2 days in the vacuum oven ( $T_g>200^\circ\text{C}$ ) .....	254

Figure 5-49: The testing setup of parylene-C creep with Heaviside temperature profile: (a) convection oven setup with a video recording apparatus, (b) parylene-C sample mounting configuration in the convection oven.....	258
Figure 5-50: Typical capture photos of the parylene-C creep test (as-deposited parylene-C tested at 120°C) after (a) 20 sec, (b) 60 sec, (c) 5 minutes, and (d) 60 minutes. (Numbers shown on the measuring ruler represent centimeters.) .....	259
Figure 5-51: Creep results of as-deposited parylene-C performed at 80°C, 100°C, 120°C, and 150°C with a Heaviside temperature profile.....	261
Figure 5-52: Creep results of parylene-C pre-annealed at 100°C in the air, performed at 80°C, 100°C, 120°C, and 150°C with a Heaviside temperature profile.....	263
Figure 5-53: Creep results of parylene-C pre-annealed at 100°C in the vacuum, performed at 80°C, 100°C, 120°C, and 150°C with a Heaviside temperature profile...	264
Figure 5-54: The stress relaxation test of polymers: (a) constant applied strain during the stress relaxation test at a constant temperature, (b) the corresponding stress output versus time.....	265
Figure 5-55: The results of constant strain-rate tests .....	277
Figure 5-56: The results of cyclic loading/unloading tests .....	278
Figure 5-57: The results from the abrupt strain-rate change tests .....	278
Figure 5-58: The results of creep tests of parylene-C film under different loading stresses: Theoretical Burger's model shows good fitting for the applied stress less than 30 MPa.....	279
Figure 5-59: The results of stress relaxation tests. Stress relaxation is observed for all the chosen strains. Higher strain gives faster stress relaxation.....	280



## LIST OF TABLES

Table 1-1: Some current typical glaucoma medications and their corresponding possible side effects .....	3
Table 1-2: History of glaucoma drainage device development [12].....	8
Table 1-3: Contemporary glaucoma drainage devices (GDDs) [12, 20] .....	9
Table 1-4: A comparison of some of current commercially available “tube-and-plate”-type glaucoma drainage devices (GDDs) [12, 20].....	14
Table 1-5: Literature review of glaucoma drainage devices (GDDs) (1969–2002) [19, 20, 73, 74] .....	16
Table 2-1: Measured cracking pressures of four single check-valves and the assemblies of multiple check-valves .....	51
Table 2-2: Cracking pressure of parylene check-valves under different releasing procedures: (1) acetone and IPA soak followed by air drying, (2) HF dip, water rinse, followed by air drying, (3) soak in a mixture of acetone and silicone oil before air drying. Zero stiction means that the stiction is too small to be measured effectively. ....	76
Table 2-3: Comparison of different slanted tether parylene-C NC check-valves introduced in this chapter. Water was used as the working fluid. ....	80
Table 3-1: Cracking pressures of two GDD systems obtained from <i>in vitro</i> and <i>ex vivo</i> tests .....	109
Table 4-1: Dimension of the new IOP sensor and its measured electrical parameters...	132
Table 4-2: Measured quality factors with different isolation layers covered on top .....	137

Table 5-1: Table of thermal coefficients of expansions obtained in different states of the parylene-C film. The literature values are also listed for comparison..... 153

Table 5-2: Derived TCEs from six cycles shown in Figure 5-5 and Figure 5-6..... 158

Table 5-3: Measured atom percentage of chlorine, carbon, and oxygen for different oxidative parylene-C films ..... 162

Table 5-4: Measured initial (after 1 hour oxidation) oxygen uptake rate for parylene-C by Nowlin [189]..... 168

Table 5-5: A list of calculated parameters using the in situ XRD measurement results of parylene-C consecutively annealed at 100°C in helium ..... 176

Table 5-6: A list of calculated parameters based on the in situ XRD measurement of parylene-C consecutively annealed at different temperatures in helium..... 179

Table 5-7: The lists of the parameters of the crystallization of parylene-C individually annealed at 100°C for different annealing times ..... 182

Table 5-8: XRD results of two as-deposited parylene-C films deposited at 22 mTorr and 35 mTorr, respectively..... 183

Table 5-9: Some of the previous published parylene-C  $T_g$  characterizing results..... 189

Table 5-10: Measured elastic modulus and temperature range of glassy, transition, and rubbery regions ..... 192

Table 5-11: Measured glass transition temperature *via* DMA approach ..... 204

Table 5-12: Measured mechanical properties of parylene-C film’s uniaxial tensile test 212

Table 5-13: Measured mechanical properties obtained at different testing temperatures ..... 222



Table 5-14: Burger's model curve fitting results of the creep and stress relaxation behaviors of as-deposited parylene-C deposited at 22 mTorr ( $T_g=53.4^\circ\text{C}$ )	241
Table 5-15: Burger's model curve fitting results of the creep and stress relaxation behaviors of as-deposited parylene-C deposited at 35 mTorr ( $T_g=55.1^\circ\text{C}$ )	243
Table 5-16: Burger's model curve fitting results of the creep and stress relaxation behaviors of parylene-C annealed at $100^\circ\text{C}$ for 30 minutes in the convection oven ( $T_g=108.2^\circ\text{C}$ ).....	245
Table 5-17: Burger's model curve fitting results of the creep and stress relaxation behaviors of the parylene-C annealed at $100^\circ\text{C}$ for 1 day in the convection oven ( $T_g=111.8^\circ\text{C}$ ).....	247
Table 5-18: Burger's model curve fitting results of the creep and stress relaxation behaviors of the parylene-C annealed at $100^\circ\text{C}$ for 1 day in the vacuum oven ( $T_g=113.1^\circ\text{C}$ ).....	249
Table 5-19: Burger's model curve fitting results of the creep and stress relaxation behaviors of the parylene-C annealed at $100^\circ\text{C}$ for 2 days in the vacuum oven ( $T_g=115.2^\circ\text{C}$ ).....	251
Table 5-20: Burger's model curve fitting results of the creep and stress relaxation behaviors of the parylene-C annealed at $200^\circ\text{C}$ for 1 day in the vacuum oven ( $T_g>200^\circ\text{C}$ ).....	253
Table 5-21: Burger's model curve fitting results of the creep and stress relaxation behaviors of the parylene-C annealed at $200^\circ\text{C}$ for 2 days in the vacuum oven ( $T_g>200^\circ\text{C}$ ).....	255

Table 5-22: Time constant of as-deposited parylene-C samples tested at different temperatures.....	262
Table 5-23: Parameters of Burger's model for creep. At 40 MPa, the sample breaks and no creep could be recorded. ....	281
Table 5-24: Parameters of Burger's model for creep recovery.....	281
Table 5-25: Parameters of Burger's model for stress relaxation .....	281