# WOUND HEALING ON ARTIFICIAL EXTRACELLULAR

## MATRIX PROTEINS

Thesis by

Eileen Fong

In Partial Fulfillment of the Requirements

For the Degree of

Doctor of Philosophy



California Institute of Technology

Pasadena, California

2010

(Defended June 2, 2010)

© 2010

Eileen Fong

All Rights Reserved.

To my family and friends

#### Acknowledgements

I would like to express my greatest gratitude to my advisor, David A. Tirrell, without whom this thesis would not have been possible. Dave is one of the most brilliant scientists I have ever met, and I am honored to have worked with him. Dave constantly amazes me with his quick-wit and foresight; yet he is exceptionally humble. Dave has inspired me tremendously with his passion for science, and has made graduate school memorable (really!). He has not only taught me to be better scientist, but also how to be a better person. I am grateful for all the guidance and support he has provided me throughout my years at Caltech. I truly enjoyed my interactions with him, and will treasure our many conversations about science and life. I will continue to hold him as my role model as, and to inspire my students the way he has inspired me. Most importantly, I am going to miss his humor.

I also had the pleasure to collaborate with Prof. Guo Chin-lin, an outstanding scientist, teacher, and friend. I am inspired by his intelligence and creativity, and have enjoyed collaborating with him and members of his lab. I enjoyed the many discussions we have had about science and life. I am grateful for his guidance and friendship, without which the last two chapters of my thesis would not have been possible.

My committee members have provided valuable advice and have helped me to become a better scientist. I would also like to thank my committee members: Prof. Marianne Bronner-Fraser has been extremely kind and she has not only introduced me to Developmental Biology, but single-handedly ignited my interest in the field of wound healing. Prof. Anand Asthagiri has taught me to connect between math and biology in his class, as well as provided valuable critique on my research. And to Prof. Mark E. Davis who was an exemplary role model for young scientists like myself.

My graduate life has been made memorable (and fun!) by many friends and colleagues at Caltech. In particular, I thank Beverly Lu and Shelly Tzlil for their life-long friendship and contributing to fond memories of my 5 years at Caltech. I also like to thank Stacey Maskarinec, who selflessly taught me everything she knew about cloning and expressing the aECM proteins. I would also like to thank all past and present members of the Tirrell laboratory, who have contributed in one way or another to making my stay here at Caltech memorable. I would also like to thank members of the Guo and Asthagiri lab for the friendship and generous support they have given me throughout the years.

I would also like to thank my family for their love and sacrifices they have made for me to pursue my dream. I am grateful for their patience and constant support, for being with me all these years. I would also like to thank Benny Poon for the years of laughter and being part of my memories at Caltech.

Lastly, I would like to acknowledge the Nanyang Technological University, Singapore (NTU) for their generous funding for 4 years at Caltech. I am also grateful to many mentors at NTU, who have provided me with valuable advice and support in my academic career at NTU.

# WOUND HEALING ON ARTIFICIAL EXTRACELLULAR MATRIX PROTEINS

June 2010

Eileen Fong, B. Mat. E., Nanyang Technological University, Singapore

Ph.D., California Institute of Technology

Supervised by David A. Tirrell

### Abstract

Collective cell migration is a key process in tissue repair, and in drawing parallels from complex multi-cellular events such as tumor morphogenesis and embryogenesis. Mechanisms of wound healing have been studied extensively *in vitro*. Extracellular matrix (ECM) is required to support cell migration and ensure rapid coverage of the wound area. The main challenge in designing biomaterials for tissue repair is to provide cells with the appropriate biological and mechanical cues. Hence, understanding key cell-ECM interactions during wound healing is necessary for effective biomaterial design.

Genetic engineering provides a convenient avenue to customize materials for any given application. The artificial protein-based biomaterials discussed in this work were derived from fibronectin and elastin. These proteins have a modular design, and have material properties that can be fine-tuned according to specific applications. The artificial extracellular matrix (aECM) proteins prepared by previous members of our laboratory have been shown to promote attachment of endothelial cells. In this work, we studied extensively epithelial and fibroblast wound healing behavior on these aECM biomaterials.

Crosslinked aECM protein films of varying RGD densities have been prepared by mixing aECM proteins with the RGD cell binding domain with aECM proteins containing the scrambled RDG sequence. Corneal epithelial wound healing was observed on aECM films with 100% RGD but not on aECM films with 2.5% RGD. Surprisingly, we found a five fold difference between the wound closure rates between these surfaces, but individual cell speeds did not increase significantly. We proposed that the five fold increase in wound closure rate was determined by the rate of crossing the boundary between the wound area and the area underneath the cell sheet. Both simulation and experimental data verified that the rate of boundary-crossing was sufficient to account for five-fold difference in wound closure rates between 100% RGD and 2.5% RGD surfaces.

Full-length fibronectin domains have also been incorporated to improve the overall cell binding properties of the aECM proteins. The aECM proteins containing full-length fibronectin domains were shown to facilitate rapid spreading of Rat-1 fibroblasts. The aECM protein containing both fibronectin domains 9 and 10 exhibited an increased binding affinity to the  $\alpha_5\beta_1$  integrin. More importantly, these aECM proteins also promoted rapid wound closure, which was comparable to that on fibronectin. We showed that aECM proteins containing full-length fibronectin domains also promoted higher

phosphorylated levels of focal adhesion kinase (FAK) and extracellular signal-regulated kinase (ERK), consistent with the faster cell migration and proliferation observed.

To try to understand how cells select wound healing mechanisms, wound healing of Madin-Darby Canine Kidney (MDCK) epithelial cells were examined *in vitro*. On surfaces containing the aECM protein bearing the fibronectin domain 10, characteristic healing patterns were observed in MDCK wound healing. These patterns are defined by the formation of leader cells at regular intervals of actomyosin purse strings. The spacing between consecutive leader cell groups was also found to be independent of the wound diameter. This spacing however, was found to decrease with increasing myosin II inhibition. These observations could be explained using a simple force transmission mechanical model. Consistent with the model predictions, we demonstrated that wounds with a zigzag geometry biased the selection of the wound healing mechanism along the wound edge. These zigzag wounds also healed nearly eight fold faster than wounds with straight edges.

## **Table of Contents**

| Abstract                   |     |
|----------------------------|-----|
| List of Figures and Tables | xii |

## 1 Introduction

| 1.1 | Wound healing  | . 1 |
|-----|--|-----|
| 1.2 | Challenges in tissue regeneration                    | . 2 |
| 1.3 | Artificial proteins as biomaterials                  | . 3 |
| 1.4 | Methods for studying wound healing in vitro          | . 5 |
| 1.5 | Thesis organization and description of contributions | . 6 |
| 1.6 | References   | 9   |

#### 

| 2.1    | Introduction                   | 13   |
|--------|--------------------------------|------|
| 2.2    | Materials and methods          | .14  |
| 2.3    | Results and discussion         | . 22 |
| 2.4    | Conclusions                    | . 33 |
| 2.5    | Acknowledgements               | 34   |
| 2.6    | References                     | 34   |
| Additi | onal information for Chapter 2 | . 36 |

| 3 | Artificia | l extracellular matrix proteins for rapid wound healing |    |
|---|-----------|---|----|
|   | Abstr     | act   | 54 |
|   | 3.1       | Introduction  | 55 |
|   | 3.2       | Materials and methods                                   | 57 |
|   | 3.3       | Results and discussion                                  | 64 |
|   | 3.4       | Conclusions   | 76 |
|   | 3.5       | Acknowledgements  |    |
|   | 3.6       | References  |    |

## 4 Early patterns in wound healing

| Abstr | act                             | . 79 |
|-------|---------------------------------|------|
| 4.1   | Introduction                    | . 80 |
| 4.2   | Materials and methods           | . 81 |
| 4.3   | Results and discussion          | . 87 |
| 4.4   | Conclusions                     | . 95 |
| 4.5   | Acknowledgements                | . 95 |
| 4.6   | References                      | . 95 |
| Addit | ional information for Chapter 4 | 97   |

## 5 Harnessing the purse string for accelerated wound healing

| Abstr | act                   | 107 |
|-------|-----------------------|-----|
| 5.1   | Introduction          |     |
| 5.2   | Materials and methods | 110 |

| 5.3 | Results and discussion | 112 |
|-----|------------------------|-----|
| 5.4 | Conclusions            | 118 |
| 5.5 | Acknowledgements       | 119 |
| 5.6 | References             | 119 |
|     |                        |     |

| 6 | Conclusions and future work |  | 20 | ) |
|---|-----------------------------|--|----|---|
|---|-----------------------------|--|----|---|

DNA plasmid maps

# List of Figures and Tables

## 1 Introduction

| 1.1 | Amino acid sequence of aECM      | proteins 4 | ļ |
|-----|----------------------------------|------------|---|
|     | i minio della seguenee or delent |            | 1 |

## 2 The Role of Boundary Crossing in Epithelial Wound Healing

| 2.1 | HCE cell spreading behavior on various substrates   |
|-----|---|
| 2.2 | (A) Schematic of wound healing experiment   |
|     | (B) Time course of wound healing on 2.5% RGD and 100% RGD substrates  |
|     | (C) Schematic of the Monte-Carlo simulation   |
| 2.3 | Wound healing behavior observed in experiments and simulations  |
| 2.4 | Image of typical substrate with an interface imaged by atomic force   microscopy   31                                 |
| 2.5 | Interface crossing and simulated and experimental rate constants of interface crossing                                |
| A1  | Amino acid sequences of aECM proteins containing (A) RGD and (B) RDG cell-binding domains                             |
| A2  | Rate constants of interface crossing, <i>k<sub>c</sub></i> from 100% RGD to various test surfaces                     |
| A3  | A schematic illustration of the cell spreading and retraction model   |
| A4  | The fit of the experimental spreading data to the theoretical expression for the relative spreading rate, Equation 10 |
| A5  | An illustration of the proliferation kinetic scheme   |

| A6   | Schematic diagram of cell at an interface, showing two possible outcomes 48     |
|------|---|
| A7   | The rate constants of interface crossing from FN to test surfaces obtained from |
|      | simulation  |
| Tabl | A1 Summary of the rates for 100% and 2.5% RGD surfaces                          |

### 3 Artificial Extracellular Matrix Proteins for Rapid Wound Healing

| 3.1 | Amino acid sequences of the aECM proteins containing full length fibronectin    |
|-----|---|
|     | domains   |
| 3.2 | Coomassie SDS-PAGE gel of purified aECM proteins                                |
| 3.3 | Time course of cell spreading of Rat-1 fibroblasts on adsorbed protein          |
|     | surfaces  |
| 3.4 | Time course of cell spreading of Rat-1 fibroblasts on crosslinked protein       |
|     | surfaces  |
| 3.5 | Binding of $\alpha_5\beta_1$ integrin to fibronectin and aECM proteins by ELISA |
| 3.6 | Quantification of wound healing behavior on adsorbed protein surfaces           |
| 3.7 | Determination of FAK and ERK phosphorylation in Rat-1 fibroblasts on various    |
|     | surfaces  |

### 4 Early patterns in wound healing

| 4.2  | Design of micropatterned PDMS blocks for creating circular and             |     |
|------|--|-----|
|      | zigzag-shaped wounds   | 83  |
| 4.3  | Schematic of wound healing assay   | 85  |
| 4.4  | Removal of PDMS preserved aECM protein surface underneath                  | 88  |
| 4.5  | Time-lapse images of MDCK wound healing behavior on both aECM and          |     |
|      | untreated glass substrates   | 89  |
| 4.6  | Verification of leader cells and purse-string structures                   | 90  |
| 4.7  | Quantification of wound healing behavior for circular wounds of increasing |     |
|      | diameters  | 91  |
| 4.8  | Effect of myosin inhibition on leader cell formation                       | 92  |
| 4.9  | Schematic of proposed mechanical model                                     | 93  |
| 4.10 | Wound curvature bias wound closure mechanisms                              | 94  |
| B1   | Model predictions  | 103 |

# 5 Harnessing the purse string for accelerated wound healing

| 5.1   | Schematic of wound closure in zigzag wounds and the effect of angles on |     |
|-------|---|-----|
|       | purse string contractions   | 109 |
| 5.2   | Initial wound geometry determines mode of wound healing                 | 113 |
| 5.3   | Time course of wound healing for zigzag wounds                          | 115 |
| Table | Wound closure rates as a function of $2\theta$                          | 116 |
| 5.4   | Overall contractile speed of purse string as a function $2\theta$       | 117 |